# Past / Future in Scintillation

#### Lecture: Hans-Jürgen Wollersheim

e-mail: h.j.wollersheim@gsi.de







### Past / Future in Scintillation

#### High energy astrophysics

Correlate the detected photon to source object as known from more precise observations in other wavelength

#### Biomedical research

Precise localization of radioactive tracers in the body Cancer diagnosis Molecular targeted radiation therapy Monitor changes in the tracer distribution → dynamic studies

#### National security

Nuclear non-proliferation / nuclear counter terrorism Contraband detection Stockpile stewardship Nuclear waste monitoring and management

#### Industrial non-destructive assessments

Determination of the material density distribution between the source and detector









# Past / Future in Scintillation

#### Afterglow = *phosphorescence*



Phosphorescence is a property of many crystals and organic materials

# Light is produced by deexcitation of molecules





# Zinc Sulfide ZnS(Ag) Scintillation Material

1866 – Theodore Sidot reported the phosphorescence of ZnS.
1002 William Creative invented a device called a printherize

1903 – William Crookes invented a device called a spinthariscope with a ZnS screen to see scintillations from α-particles.







In 1903 W. Crookes demonstrated in England his "spinthariscope" for the visual observation of individual scintillations caused by α-particles impinging upon a ZnS screen. In contrast to the analogue methods of radiation measurements in that time the spinthariscope was a single particle counter, being the precursor of scintillation counters since. In the same period F. Giesel, J. Elster and H. Geitel in Germany also found that scintillations from ZnS represent single particle events. This paper summarizes the historical events relevant to the advent of scintillation counting.

A spinthariscope from 1904. Height about 5 cm, Ra-source (A), ZnS screen (B), magnifying glass



# Zinc Sulfide ZnS(Ag) Scintillation Material

✤ 1944 – photomultiplier tube was invented





✤ 1948 – H. Kallmann



# History of Scintillators

History of scintillators starts short after the discovery of X-rays at the end of 19<sup>th</sup> century





# Compton Suppression Shields NaI(Tl) versus BGO

| material                          | NaI(Tl)         | BGO               |
|-----------------------------------|-----------------|-------------------|
| density (g/cm <sup>3</sup> )      | 3,67            | 7.13              |
| 50% attenuation for 662 keV in cm | 2.5             | 1.0               |
| Index of refraction n             | 1.85            | 2.15              |
| Emission (photons/keV)            | 38              | 8                 |
| Decay time (ns)                   | 250             | 300               |
| Maximum size grown (mm)           | 700             | 75                |
| Radioactive contamination         | <sup>40</sup> K | <sup>207</sup> Bi |







# Heidelberg – GSI Crystal Ball





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# **Tomographic Imaging**



PET





SPEC

СТ

OPTICAL

MRI



# **Computed Tomography**

- CT scanning (originally known as CAT)
- X-rays taken at a range of angles around the patient
- Generation of 3D images





# **Positron Emission Tomography**





# Positron emission tomography





# Single Photon Emission Computed Tomography



- Most commonly used tracer in SPECT is  ${}^{99}$ Tc<sup>m</sup>, 140 keV a pure single photon emitter T<sub>1/2</sub> = 6.02 h.
- Utilizes a gamma-ray camera rotated in small ~3<sup>o</sup> steps around the patient.



# The motivation behind the project



- Existing technology relies on BGO scintillator technology
  - Limited position resolution
  - High patient dose requirement.
  - Poor energy resolution only accept photopeak events.
  - Will not function in large magnetic field
- SPECT applications utilizing Compton Camera techniques.



- **\therefore** Excellent resolution  $\Delta x = 2 \text{ mm}$
- Large field of view (FOV) = 8x9 cm<sup>2</sup>
  - Large FOV of ~20 cm diam.
  - Low spatial resolution 0.5-1 cm







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# Gamma Camera: Individual multi-anode readout

16 wires in X axis and 16 wires in Y axis





Photocathode = 56.25 mm

C.Domingo Pardo, N. Goel, et.al., IEEE, Vol.28, Dec. 2009



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Pushpendra P. Singh & Hans Jürgen Wollersheim (2018)

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# Scanner at GSI



#### Position sensitive detector

#### Characteristics:

- Faster
- Precision: 1-2 mm
- Imaging capability

#### **Rotating table**

#### **Requirements:**

- 1. Position sensitive detector
  - Excellent  $\Delta x/x$
  - Large field of view
- 2. Method to compare the pulses



• Determine:  $X_r(x_m, y_m), Y_r(x_m, y_m)$ 





#### Gamma-ray scattering technique





### Position reconstruction



C. Domingo Pardo, N.Goel, et.al., IEEE, Dec. 2009 Volume: 28 Issue 12

C.W.Lerche, et.al., NIM A, Vol 537, pp. 326-330, Jan. 2005



# Position reconstruction



Field of view =  $28 \text{ cm}^2$ 

Average spatial resolution in X and Y ~ 1mm

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### Superiority over conventional scanner

coincidence between the Germanium and BGO detectors for 90 degree Compton scattered events for depth determination



Advantage over conventional scanner: Full detector can be scanned in one measurement 10 times faster than a conventional scanner Accuracy of simulations can be checked for complex regions of electric field



# Scanner based on pulse shape comparison scan







### Scanner based on pulse shape comparison scan



### Pulse shape comparison scan method based on a position sensitive detector



# $\chi^2$ minimization method





# Characterization of planar HPGe detector





#### t = 2 cm







Position sensitive detector



#### Front view (0 deg):



Side view (90 deg):













### **Detector scan**

### Front view (0 deg):



Side view (90 deg):













### Planar HPGe detector scan

Intensity distribution for photopeak events



# Outlook



The GSI system uses conventional NIM and VME electronics, which makes it not easily portable, not easily scalable and rather expensive if one wants to build many of these devices.

However, this drawback could be overcome thanks to the increasing technology of electronics, e.g. a new acquisition system based on ASIC, FPGA, etc. technologies. This would also make the system more suitable for medical applications.







128-channel analogue pipeline chip

M.J. French et al., NIMA 466 (2001) 359



# **Position Extraction in Planar Detectors**

Y (orthogonal direction)







Position resolution of <0.5mm achieved at 122 keV in all three dimensions.



#### LLNL- Double Sided Strip Detectors (DSSD) built of high-purity Ge and Li-drifted Si for gamma-ray imaging applications

(Ethan Hull, LLNL, Paul Luke, LBNL, and Davor Protic, Research Center Juelich, Germany)



2x38 strip DSSD HPGe detector with 2 mm pitch and 11mm thickness



2x32 strip DSSD Si(Li) detector with 2 mm pitch and 10mm thickness



# Gamma-Ray Imaging



Conventional detectors accept gamma-rays from all directions and can be overwhelmed by local backgrounds.

